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Reply to the Editor:

We would like to thank Drs Asano and Okita for their comments regarding our study,¹ in which we demonstrated that the majority of arch aneurysms could be repaired with a long elephant trunk (LET) anastomosed at the base of the innominate artery without distal anastomosis in the descending aorta. They raised the issue of distal fixation of the LET in our technique. Although the proximal end of the LET is sutured at the base of the innominate artery and proximal endoleak is prevented, the distal end of the LET is not fixed, and distal endoleak is possible with our method. As demonstrated in Figure 2, C, in our article, the aneurysmal sac outside the LET was enhanced with contrast material in 9% of our patients, and they required distal fixation of the LET.

However, it is important to note that the majority (91%) of our patients did not show contrast material outside the LET, and none had expansion or rupture of the aneurysm occur during the average follow-up of 33 ± 18 months. Furthermore, it was encouraging for us to find that the nonenhanced aneurysmal sac around the LET shrank more than 5 mm in 82% of the patients and more than 10 mm in 50% at 1 year after total arch replacement with the LET, as shown in Figure 2, B, of our article. The follow-up period might not have been long enough to rule out the possibility of late expansion of a nonenhanced aneurysm, and we consider that long-term follow-up of our patients is mandatory.

In their letter they referred to their article,² in which they insist that arch aneurysms with extension to 1 cm below the level of the carina are accessible from a median sternotomy. Interestingly, they demonstrate that an increased depth of distal anastomosis is a risk factor for prolonged distal anastomosis, even in Japanese patients, whose chest cavities are generally smaller than those in white patients.² Based on my personal experience as a clinical fellow for 3 years in United States, I wonder how many surgeons are comfortable to do the distal anastomosis 1 cm below the level of the carina in a typical barrel-chested white patient. On the other hand, with our technique, the descending aorta in the deep

posterior mediastinum does not need to be exposed, but rather only a distal anastomosis is performed in the distal ascending aorta. Because of this simplicity, we required only 23 ± 8 minutes of hypothermic circulatory arrest in the lower body to complete the insertion and anastomoses of the LET. Thus we conceive that the benefit of our technique might be even more evident in white patients with a large chest.

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Tissue-engineered heart valves: Bioreactor—yes or no?

To the Editor:

I read with great interest the article by Vincentelli and associates.¹ In this article the authors present the results of the effects of in situ injection of autologous bone marrow-derived mononuclear cells and mesenchymal stem cells (MSCs) on the outcome of xenogenic decellularized scaffolds in a lamb model. The main focus of this article is on a new method to reseed the cells in valve scaffolds consisting of an in situ injection of bone marrow cells into a porcine decellularized scaffold before implantation. Tissue-engineered heart valves created from MSCs and injected directly in a decellularized xenograft scaffold exhibited satisfactory hemodynamic aspects after 4 months.

Even if the authors demonstrate that in the MSC group the global organization of collagen fibers was preserved, a few fusi-

form cells were observed in the subendothelial area and the adventitia.

Pulmonary leaflets present few recolonizing cells positive for α -actin staining, with a typical organization in 3 layers, fibrosa, spongiosa, and ventricularis, as previously reported by others,² who showed that decellularized pulmonary valves revealed a well-preserved 3-dimensional network of collagen fibers in the extracellular matrix.

As we know, maintenance of the structural valve properties is fundamental to preserve the extracellular matrix with its complex of glycosaminoglycans and collagen fibers produced from valve fibroblasts and active fibroblasts. This appears to be fundamental for the mechanical valve's capability and its long-term durability.²⁻⁴ Repopulation of a decellularized valve is crucial for valve vitality. How this could be achieved still remains controversial. As a matter of fact, at this time, it is not completely clear whether a bioreactor is fundamental for the valve repopulation. Lichtenberg and colleagues⁵ clearly demonstrated that in vitro conditioning of engineered tissues in a bioreactive system stimulates and enhances the production of extracellular matrix and the related tissue strength. On the contrary, Dohmen and associates,⁶ studying seeded or nonseeded decellularized valves implanted into right ventricular juvenile sheep outflow tracts, showed that a difference was identified in the recellularization density of in vitro seeded and nonseeded valves up to 3 months, but no such difference was seen after 6 months.

Nevertheless, a moderate pulsatile flow with small increments seems to be able to stimulate endothelial cell proliferation on the decellularized valve scaffold. A rapid increase in bioreactor flow to physiologic levels leads to significant damage of the reseeded endothelium and complete loss of cusp cellularity. This effect might be responsible for the in vivo failure of static, reseeded, tissue-engineered valves exposed to physiologic hemodynamic forces.

However, whether MSCs injected in the scaffold induced in situ differentiation into myofibroblasts and endothelial cells remains uncertain. The injection of the stem cells in the inner side of the valve before valve implantation must be able to produce a colonization not only by recipient endothelial cells but above all by active